Dependence of the Vulnerability Index on the Heart Cycle Length

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Summary

Index of vulnerability is a parameter based on ventricular gradient evaluating the risk of arrhythmia development. The index is derived from isointegral maps of the QT interval. Individual characteristics of isointegral maps are influenced by different factors, which contribute to the relatively high variability among measured parameters of maps in measured subjects. While several electrocardiographic indexes have been introduced, there are only few studies of their dependence on heart rate. In this study we set out to establish the dependence of vulnerability index on the RR interval or heart rate in healthy population. A positive linear correlation between RR intervals and mean and minimum values of vulnerability indexes was found.

Key words
Body surface potential • Heart rate • Ventricular gradient • Isointegral map • Vulnerability index • RR interval

Introduction

Heart rate can influence the risk of arrhythmia development since it probably influences the dispersion of duration of the action potential (APD) across the heart. Experimental studies confirmed a significant increase with cycle length prolongation for transmural dispersion (Antzelevitch et al. 1999).

Electrocardiographic body surface mapping offers the possibility for evaluation of the risk of development of arrhythmia. It can be simply the number of extrema in the QRST isointegral map (IIM, Gardner et al. 1986, Martinka 2006) or more sophisticated, vulnerability index based on comparison of IIM QRST of a test subject with IIM QRS and IIM ST-T of a control (Urie et al. 1978). We wanted to find out whether there is any correlation between the vulnerability index changes and the heart rate of the examined person.

Methods

We constructed IIM QRS, IIM ST-T and IIM QRST for 106 young people of 18–25 years of age (47 women, 59 men). None had a history of cardiovascular disease and they had ECG without pathological changes. We calculated the vulnerability indexes for each subject as a test, while all other subjects served as controls.

Data for body surface mapping were registered using the limited 24-lead system after Barr (Barr et al. 1971) and processed using the ProCardio mapping
system (Rosík et al. 1997). Data were registered in supine position. Linear baseline was taken through TP segments. The onset and offset of the QRS complex and the T wave was established manually from the root mean square signal (Kozlíková 1990). Isointegral maps were constructed as distributions of potential time integrals over chosen time intervals.

The vulnerability index is constructed using IIM QRST as follows: IIM QRST of the subject to be tested is compared with all subjects of the control group and the best matching map is determined (the map with the smallest total QRST area difference of all leads). The difference between the test map and the best match from the control group is shown as the “vulnerability map” according to the following equation for each point of the map:

\[ V = IIM\ QRST_{test} - (IIM\ QRST_{control} + \alpha \cdot IIM\ ST-T_{control}) \]  

(1)

where \( \alpha \) is determined by minimizing the squared difference:

\[ \frac{d(V^2)}{d\alpha} = 0 \]  

(2)

Coefficient \( \alpha \) has to fulfill the condition:

\[-1 \leq \alpha \leq 1 \]  

(3)

The vulnerability index VI is calculated as the square root of the sum of the squares of all values contained in the vulnerability map

\[ VI = (\sum Vi^2 / n)^{1/2} \]  

(4)

where \( V_i \) is the value of vulnerability map in the \( i \)-th point, \( i = 1, 2, ..., n \).

In an ideal situation, the same subject may serve as a test (under arrhythmic conditions) and as a control (under physiological conditions). In practice, this is usually not possible. Therefore, the best matching map of a different control subject serves for comparison. In this study we used the minimum vulnerability index (\( V_{I_{\min}} \)), which is the lowest value of VI obtained from all comparisons of the tested subjects with control subjects, and mean vulnerability index (\( V_{I_{\text{mean}}} \)), which is the average value of all comparisons of the tested subjects with control subjects. Each comparison that was in compliance with equations (1) and (2) was considered.

Therefore, the aim of this study was to find out whether there exists any correlation between the vulnerability index and the RR interval duration representing the heart rate.

**Results**

The average value ± standard deviation of the RR interval was 872 ± 114 ms (the corresponding heart rate was 69.9 ± 8.7 bpm). The average value of the \( V_{I_{\min}} \) was 9.45 ± 5.00 mV.ms, for the \( V_{I_{\text{mean}}} \) it was 15.81 ± 5.15 mV.ms.
The vulnerability index in both cases increased with increasing value of the RR interval. We found statistically significant linear correlations between \( VI_{\text{min}} \) and RR (Fig. 1)

\[
VI_{\text{min}} = -12.12 + 0.025 \times RR
\]

with correlation coefficient \( r = 0.562 \).

and between \( VI_{\text{mean}} \) and RR (Fig. 2).

\[
VI_{\text{mean}} = -1.0049 + 0.0195 \times RR
\]

with correlation coefficient \( r = 0.386 \). A better fit for \( VI_{\text{mean}} \) was the exponential dependence

\[
VI_{\text{mean}} = \exp(1.671 + 0.0012 \times RR)
\]

with correlation coefficient \( r = 0.392 \) (no statistically significant difference against the linear dependence).

**Discussion**

The value of VI depends only on the repolarisation sequence and does not depend on the depolarisation sequence (Urie et al. 1978). Previous studies showed that the dependence of QT interval on the RR interval is linear (Smetana et al. 2004). If the heart rate was influenced only by the action of the sinoatrial node, it would not necessarily cause any increase of the ventricular gradient. However, if a lower heart rate increases the dispersion of action potential duration across the heart, it can also change the repolarization sequence, which can increase the risk of arrhythmia development. It was found that the prolongation of the cycle length was linked to the occurrence of Torsade de pointes as well as to the QT interval prolongation at slow heart rates (Sicouri and Antzelevitch 1991), which is in accordance with our results.

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**References**


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