Mismatch of Local Blood Flow and Oxidative Metabolism in Stunned Myocardium

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Summary

Myocardial blood flow is spatially heterogeneous, reflecting nonuniform oxygen supply. Also, myocardial oxidative metabolism is spatially heterogeneous. The effects of acute ischemia and reperfusion on the relationship between local myocardial blood flow (LMF) and oxidative metabolism are still unknown. LMF was measured in isolated, blood-perfused rabbit hearts using colored microspheres and oxidation water labeled with ¹⁸O₂ (H₂¹⁸O). Three protocols were performed: ¹⁸O₂-perfusion during normoxia (N; n=7), during early reperfusion (ER; 10 min, n=6), and late reperfusion (LR; 40 min, n=6) following 20 min no-flow ischemia. LMF and local H₂¹⁸O residues were determined within defined myocardial samples (105 ± 15 mg). For interindividual comparison, values were normalized to the mean of the individual experiment and expressed as percentages. LMF ranged from 18 to 193 % (N), 12 to 250 % (ER), and 11 to 180 % (LR). The H₂¹⁸O tissue residue ranged from 63 to 132 % (N), 73 to 142 % (ER) and 32 to 148 % (LR). The correlation between LMF and local oxidative metabolism during N (r=0.77; n=56) was lost in the postischemic heart during ER and LR. LMF during N and ER were only weakly correlated (r=0.24; n=48), whereas LMF during N and LR correlated well (r=0.87; n=48). It is concluded that the heterogeneous LMF pattern at baseline is maintained in the stunned myocardium whereas that of local oxidative metabolism is not. Apart from the established mechanisms underlying myocardial stunning, a mismatch between local flow and oxidative metabolism might also contribute.

Key words

Myocardial stunning • Local blood flow • Local oxidative metabolism • Perfusion-metabolism mismatch • Heterogeneity

Introduction

Local blood flow within mammalian myocardium is heterogeneously distributed: it varies between 20 % of the mean in low-flow areas and 200 % in highflow areas (Deussen *et al.* 1996, King *et al.* 1985, Sonntag *et al.* 1996). The reversible myocardial dysfunction that follows brief periods of ischemia, i.e. myocardial stunning (Heyndrickx *et al.* 1975, Bolli 1990) is more pronounced in areas where the preceding ischemia is more severe (Bolli *et al.* 1989). Whereas stunning appears to be related to the preceding ischemic blood flow, there is no relation to the instantaneous blood flow during reperfusion (Thaulow *et al.* 1989). However, the

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relation of blood flow and metabolism during reperfusion has not yet been studied at the spatial resolution that is necessary for analyzing the above blood flow heterogeneity.

Recently, while measuring both local oxidative metabolism and local myocardial flow, we found a correlation between these two variables in the normoxic, buffer-perfused heart (Schwanke *et al.* 2000). In the present study, we have investigated whether or not this correlation also holds for the blood-perfused myocardium, and whether it is not altered in the stunned myocardium.

Methods

Experiments on 19 isolated hearts from adult New Zealand White rabbits (age 5 - 8 months, weight 3100 - 3800 g) were performed in accordance with the animal welfare regulations of the German authorities that adhere to the guiding principles of the Helsinki Declaration.

The hearts were connected to a modified Langendorff apparatus and perfused with a Krebs-Henseleit solution containing bovine erythrocytes (hct = 30 %; Hb = 10 g/dl), 40 g/l bovine serum albumin and 5000 IU/l heparin. The Krebs-Henseleit composition was as follows (in mM): NaCl (90), NaHCO₃ (30), KCl (4), Na₂HPO₄ (1), MgSO₄ (0.5), CaCl₂ (2.5). In addition to pyruvate (2.2 mM) and glucose (11.1 mM), the perfusate contained free fatty acids bound to albumin (1.4 mM).

This perfusate – it will be called 'blood' throughout this paper – was equilibrated with 72 % N₂, 22 % O₂, 6 % CO₂ or alternatively with 72 % N₂, 22 % $^{18}O_2$, 6 % CO₂ using an infant oxygenator (D705 Midiflow; Dideco; Mirandola, IT) and its temperature was maintained at 38 °C.

Using a servo-controlled roller pump (WM 505, Watson Marlow, Falmouth, GB), coronary arterial pressure (CAP; Statham P23, Gould Nicolet, Erlensee, DE) was adjusted to 80 mm Hg. Coronary blood flow (T206, Transonic Systems Inc, Ithaka/NY, US) and the difference in arterio-venous oxygen content (A-VOX Systems, Inc; San Antonio, TX, US) were measured in the perfusion circuit that contained a blood filter (40 μ m; AF-1040 GOLD, Baxter Bentley; Irvine, CA, US) (Fig. 1 left).



Fig. 1. Modified Langendorff ap-paratus for blood perfusion of isolated rabbit hearts. In the systemic circuit (right), left ventri-cular pressure (LVP), aortic pressure (AoP), and aortic flow (AoF) and in the perfusion circuit (left) coronary arterial pressure (CAP), global myocardial blood flow (CBF), and the difference in coro-nary arterio-venous oxygen content (AVDO₂) were measured. An op-tional gas circuit containing 22 % ¹⁸O₂ permitted labeling of cardiac oxidation water (top). A latex balloon (HSE, #12-14, H. Sachs Elektronik, March-Hugstetten, DE) was inserted into the left ventricle *via* the mitral valve. The balloon was connected to an artificial systemic circuit that was separated from the perfusion circuit. To assess ventricular function, left ventricular pressure (TC-500, Millar Instruments, Houston/TX, US) and cardiac output (T206, Transonic Systems Inc, Ithaka/NY, US) were measured in the systemic circuit (Fig. 1 right).

Blue and red microspheres (Kowallik *et al.* 1991; $\emptyset = 15 \ \mu$ m) were used to measure local myocardial blood flow (LMF). After sonication (RK156, Sonorex, Bandelin electronic, Berlin, DE) and 1 min vigorous shaking (VF1 Vibrofix, IKA-Labortechnik, Staufen i.B., DE), the spheres were injected into the perfusion line directly above the aortic root.

Experimental protocol

After excision and transfer into the Langendorff apparatus, hearts were allowed to stabilize for 15 min. In the following 15-min period, hemodynamic baseline values were assessed. At the end of each protocol, the perfusion was abruptly terminated, and the hearts were immersed into liquid nitrogen. Three different protocols were followed:

Normoxia

Following baseline measurements, normoxic hearts (n = 7) were perfused with ¹⁸O₂-equilibrated blood for 10 min (Fig. 2 top). For LMF measurement, 120,000 blue microspheres were injected 5 min prior to termination of the experiments.

Early reperfusion

Baseline measurements were followed by 20 min no-flow ischemia (n=6). During reperfusion, ${}^{18}O_2$ -equilibrated blood was used for 10 min (Fig. 2 middle). 120,000 blue microspheres were injected 5 min prior to ischemia, and 120,000 red microspheres were injected 5 min prior to termination of the experiments.

Late reperfusion

Baseline measurements and a 20 min no-flow period were followed by 30 min reperfusion. Thereafter, the hearts (n = 6) were perfused with ¹⁸O₂-equilibrated blood for an additional 10 min (Fig 2, bottom). LMF was measured as in the early reperfusion series.



Fig. 2. Protocols performed in the present study. (1) normoxia (top); (2) 10 min ¹⁸O₂perfusion in early reperfusion following a 20 min noflow ischemia (middle); (3) 10 min ¹⁸O₂-perfusion in late reperfusion following a 20 min no-flow ischemia and 40 min reperfusion (bottom).

Myocardial tissue preparation

The frozen hearts were cut into basal, median and apical transversal slices. Samples of right ventricular free wall, septum and left ventricular free wall were dissected from the slices. The basal, median, and apical portions of the left ventricular free wall were further divided into subendocardial and subepicardial layers. A total of eight tissue samples were taken from each heart, with an average weight of 105 ± 15 mg.

Water extraction, $H_2^{18}O$ processing, and local blood flow

This procedure was described in detail previously (Schwanke et al. 1994, Schwanke et al. 1996). In brief, the water was extracted from the tissue samples during 2 h of lyophilization, after which 7.5 µl aliquots were taken and converted quantitatively to CO₂ using the guanidine hydrochloride technique (Dugan et al. 1985). The oxygen isotope ratio $({}^{18}O/{}^{16}O)$ within the CO₂ samples was determined using mass spectrometry (Finnigan, MAT 251, Bremen, DE). The oxygen isotope ratios were converted from the SMOW values [‰ SMOW] (Baertschi, 1976) to SI units and expressed as local H_2^{18} O residue of cardiac tissue water per 1 g wet mass, thus representing a measure of local oxidative metabolism. Local myocardial flow was determined from the dried tissue samples by measuring the microsphereassociated colour intensity using spectrophotometry (Kowallik et al. 1991). Local blood flow data were normalized to 1 g wet mass. In all tissue samples, both local myocardial blood flow and the $H_2^{18}O$ residue were determined.

Calculations and statistics

Global myocardial oxygen consumption (MVO₂, ml·min⁻¹·g⁻¹) was calculated according to Fick's principle: $MVO_2 = CBF [ml·min⁻¹·g⁻¹] \cdot AVDO_2 [mlO_2 \cdot (100 ml)^{-1}].$ Both oxidative metabolism and local blood flow were normalized to the mean values of the individual experiment.

Hemodynamic data are presented as means \pm S.D. The relations between (a) LMF and local oxidative metabolism and (b) LMF during baseline and reperfusion were determined by linear least-squares regression analysis using SYSTAT 5-0 software (SPSS Inc, Chicago/IL, US). A p-value < 0.05 was taken to indicate statistical significance.



Fig. 3. Linear regression between local myocardial blood flow (LMF) and local oxidative metabolism (local $H_2^{18}O$ residue after 10 min ¹⁸ O_2 perfusion) within isolated, blood-perfused rabbit hearts. **Top:** Both variables correlated closely during normoxic control. The correlation coefficient (r) was equal to 0.77 (p < 0.05; n = 56 samples from 7 hearts;). **Middle:** During early reperfusion after 20 min total ischemia, LMF and local oxidative metabolism correlated less close: r = 0.20; n.s.; n = 48from 6 hearts. **Bottom:** During late reperfusion after 20 min total ischemia, the correlation between LMF and local oxidative metabolism was completely lost: r = 0.15; n.s.; n = 48 from 6 hearts).

Results

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Heart rate	124 ± 16
[min ⁻¹]	
Left ventricular pressure	105 ± 9
[mm Hg]	
Cardiac output	70 ± 11
$[ml \cdot min^{-1}]$	
Coronary flow	1.4 ± 0.5
$[ml \cdot min^{-1} \cdot g^{-1}]$	
MVO ₂	0.08 ± 0.01
$[ml \cdot min^{-1} \cdot g^{-1}]$	

Normoxia (N)

Hemodynamics and global myocardial oxygen consumption (MVO₂) are summarized in Table 1. In 56 tissue samples, local myocardial blood flow (LMF) ranged between 18 % and 193 % of the mean. Local oxidative metabolism varied between 63 % and 132 % of the mean. Linear regression analysis between both variables gave the equation: $H_2^{18}O = 0.24$ LMF + 0.75 (r=0.77; p < 0.001; n = 56; Fig. 3 top).

Early reperfusion (ER)

Ventricular function was clearly depressed, coronary blood flow was increased to fivefold, and global MVO₂ was almost unchanged (Table 2).

Table 2. Hemodynamics during control (ctr) and after 20 min no-flow ischemia during early reperfusion (rep ≤ 10 min)

	ctr	rep
Heart rate	164 ± 26	86*±13
$[min^{-1}]$		
Left ventricular	87 ± 7	$51*\pm 8$
pressure		
[mm Hg]		
Cardiac output	45 ± 6	$0*\pm 0$
$[ml \cdot min^{-1}]$		
Coronary flow	1.3 ± 0.1	$6.5* \pm 0.7$
$[ml \cdot min^{-1} \cdot g^{-1}]$		
MVO ₂	0.08	0.06 ± 0.01
$[ml \cdot min^{-1} \cdot g^{-1}]$		

*p < 0.05 vs. ctr

In 48 tissue samples, LMF ranged between 12 % and 250 % of the mean, and local oxidative metabolism ranged from 73 % to 142 %. The two variables did not correlate: $H_2^{18}O = 0.06$ LMF + 0.94 (r = 0.20; n.s.; n = 48; Fig. 3 middle). Similarly, LMF during N and ER were only weakly correlated: LMF_{ER} = 0.43 · LMF_N + 0.57 (r = 0.24; n.s.; n = 48; Fig. 4 top).

Late reperfusion (LR)

Ventricular function started to recover towards baseline values, while cardiac output was still showing signs of myocardial stunning. Coronary blood flow was only slightly lower than during baseline, whereas MVO₂ remained almost unchanged (Table 3).

In 48 tissue samples, LMF ranged between 11 % and 180 % of the mean, and local oxidative metabolism ranged from 32 % to 148 % of the mean. Linear regression analysis between both variables exhibited no correlation: $H_2^{18}O = 0.09 \text{ LMF} + 0.90 \text{ (r} = 0.15; \text{ n.s.; n} = 48; \text{ Fig. 3 bottom}$). In contrast, LMF during N and LMF during LR correlated: $LMF_{LR} = 0.86 \cdot LMF_N + 0.17 \text{ (r} = 0.87; p < 0.05; n = 48; \text{Fig. 4 bottom}$).

Table 3. Hemodynamics during control (ctr) and after 20 min no-flow ischemia during late reperfusion (rep ≥ 30 min)

	ctr	rep
Heart rate	183 ± 6	167 ± 20
$[min^{-1}]$		
Left ventricular	88 ± 5	80 ± 7
pressure		
[mm Hg]		
Cardiac output	41 ± 4	$21* \pm 10$
$[ml \cdot min^{-1}]$		
Coronary flow	2.1 ± 0.8	1.5 ± 0.5
$[ml \cdot min^{-1} \cdot g^{-1}]$		
MVO ₂	0.08 ± 0.01	0.06 ± 0.01
$[ml \cdot min^{-1} \cdot g^{-1}]$		

p < 0.05 vs. ctr

Discussion

Using myocardial samples with an average mass of 105 ± 15 mg, we were close to the optimal sample size of about 80 mg to look at blood flow heterogeneity

(Bassingthwaighte *et al.* 1989), and by recovering 500 - 6000 spheres per sample, the methodological error is estimated to be only 3 - 9 % (Dole *et al.* 1982, Nose *et al.* 1985), i.e. considerably smaller than the differences found in local myocardial blood flow (LMF), which varied by a factor of nearly 10.

The heterogeneity in LMF found in the present study was almost independent of the actual protocol and agrees well with data in the literature (King and Bassingthwaighte 1989, Bassingthwaighte *et al.* 1990, Deussen *et al.* 1996, Sonntag *et al.* 1996) and our recent study on buffer-perfused hearts (Schwanke *et al.* 2000).



Fig. 4. Linear regression between local myocardial blood flow (LMF) during normoxia and during reperfusion. **Top:** LMF during normoxic control and during early reperfusion after 20 min total ischemia were not closely correlated, indicating that the flow pattern during early reperfusion had changed compared with normoxic control: $LMF_{ER} = 0.43 LMF_N + 0.57$ (r = 0.24; n.s.; n =48). **Bottom:** LMF during normoxic control and during late reperfusion closely correlated indicating that the LMF patterns during normoxic control and during late reperfusion were similar: $LMF_{LR} = 0.86 LMF_N + 0.17$ (r = 0.87; p < 0.05; n = 48)

The spatial blood flow pattern observed at baseline changed during early reperfusion, i.e. during reactive hyperemia. Yet, after reactive hyperemia had subsided and blood flow was slightly below baseline during late reperfusion, the postischemic flow pattern was almost identical with the baseline pattern, the slope between both LMFs being only somewhat below the line of identity (Fig. 4). We have thus confirmed earlier findings (Schulz *et al.* 1991) that the dysfunction in stunned myocardium cannot be attributed to an insufficient blood flow *per se.*

Most techniques measure respiratory activity, and hence local oxygen consumption, only indirectly using labelled substrates (Breull et al. 1984, Groeneveld and Visser, 1993, Kuschinsky et al. 1993, Müller et al. 1993, Deussen and Bassingthwaighte 1996, Deussen 1997). These techniques have a major drawback (Bassingthwaighte and Goresky 1984, Deussen and Bassingthwaighte 1996), because myocardial substrate metabolism varies greatly with the physiological state. Such changes in substrate utilization occur in particular in the stunned myocardium (Renstrom and Liedtke 1995), when fatty acid oxidation recovers quickly during reperfusion and dominates as a source of oxygen consumption (Lerch 1995, Kantor et al. 1999, van de Velde et al. 2000). Our technique directly determines the transfer of oxygen to oxidation water and thus provides a direct measure of local oxidative phosphorylation activity. Hence, although the blood used in the present study contained both glucose and fatty acids, any protocol-dependent shift in substrate utilization during reperfusion will probably not have affected our results concerning oxidative metabolism.

The most direct measure of local aerobic metabolism is the local production rate of oxidation water. This rate is difficult to measure directly, and therefore the local residue of oxidation water must serve as a reasonable index of the local production rate. Since the local ¹⁸O water tissue residue depends both on intracellular production and simultaneous washout from the tissue, a mathematical model analysis (Deussen and Bassingthwaighte 1996) is necessary to calculate the local MVO₂. Such analysis, however, seemed difficult for the present study, since the permeability surface area product in stunned myocardium is not known. Therefore, the ¹⁸O water residue served as an estimate of local MVO₂ in the present study.

The correlation between local flow and oxidative metabolism at baseline was largely lost during early

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reperfusion (r = 0.20) and even worse at late reperfusion (r = 0.15). Because the flow heterogeneity during late reperfusion was similar to that during normoxia it appears that it is not the loss in flow heterogeneity but a loss in metabolic heterogeneity, which is associated with myocardial stunning, reflecting a mismatch between local flow and local metabolism.

We hypothesize that local metabolism reflects local myocardial function. Unfortunately, we can only speculate on contractile function on the microregional level (~ 80 mg) as no techniques to measure function at that resolution are available. Since low-flow / low-metabolism areas do not become necrotic with a blood flow as low as 0.2 ml·min⁻¹·g⁻¹, their local function is also expected to be low. In turn, high-flow in high-metabolism areas appears not to reflect luxury perfusion (Bassingthwaighte and Goresky 1984, King and Bassingthwaighte 1989, Deussen *et al.* 1996), and therefore their function is expected to be high.

We propose that the difference in local $H_2^{18}O$ residue between low-flow and high-flow areas reflects increased reperfusion/reoxygenation injury in postischemic high-flow areas. If so, local function in high-flow areas is very likely also more compromised than that in low-flow areas secondary, at least in part, to the decreased efficiency as a result of fatty acid oxidation at the expense of glucose oxidation. A very similar finding was reported using a different experimental approach: high-flow areas in the myocardium of baboons were more susceptible to undergo necrosis during ischemia (Ghaleh et al. 1996).

Critique of methods

One factor might have introduced an error into our results that is related to the baseline measures of the three series. We acknowledge the differences between the series and attribute them to biological variations. On the other hand, the ventricular function does not differ considerably, if expressed in terms of the rate pressure product (13,020 *vs.* 14,268 *vs.* 16,104 mm Hg/min) which nicely fits with the global MVO₂ that was almost identical in the three series. In turn, we exclude a learning curve effect, since both the protocol and the experimental model is being used in our laboratory for a long time (Schipke *et al.* 1996, Schwanke *et al.* 2000).

In conclusion

We propose that myocardial stunning is due to the functional failure of high-flow areas and the inability of low-flow areas to compensate for the functional loss. Such mismatch between local flow and metabolism may contribute to myocardial stunning.

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Reprint requests

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